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Antimicrobial and wear performance of Cu-Zr-Al metallic glass composites

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Abstract

The antimicrobial and wear behaviour of metallic glass composites corresponding to the $\text{Cu}_{50+x}(\text{Zr}_{44}\text{Al}_6)_{50-x}$ system with $x=(0, 3 \text{ and } 6)$ has been studied. The three compositions consist of crystalline phases embedded in an amorphous matrix and they exhibit crystallinity increase with increasing copper content, i.e., decrease of the glass-forming ability. The wear resistance also increases with the addition of copper as indirectly assessed from H/E , and H^3/E_r^2 parameters obtained from nanoindentation tests. These results are in agreement with scratch tests since for the alloy with highest Cu content, i.e., $\text{Cu}_{56}\text{Zr}_{38.7}\text{Al}_{5.3}$, reveals a crack increase, lower pile-up, prone adhesion wear in dry sliding and higher scratch groove volume to pile-up volume. Samples with higher Cu content revealed higher hydrophilicity. Time-kill studies revealed higher reduction in colony-forming units for *E. coli* (gram-negative) and *B. subtilis* (gram-positive) after 60 min of contact time for the $\text{Cu}_{56}\text{Zr}_{38.7}\text{Al}_{5.3}$ alloy and all the samples achieved a complete elimination of bacteria in 250 min.

1. Introduction

Nosocomial infections (i.e., hospital-acquired infections, HAI) and bacterial resistance to antibiotics are topics of utmost importance in [1]. For this reason, numerous studies about the economic and social impact of HAI have been performed over the years [2-4]. For example, a European survey from 2011–2012 estimated that the total annual number of patients with HAI in European acute care hospitals was 3.2 million [5]. The most common method to tackle this challenge in hospitals is to clean touch surfaces using chemical products. The major drawback is that the large number of touch surfaces requires considerable

financial resources to ensure proper surface sterilization. In this regard, the self-sterilizing behaviour of antimicrobial materials makes them an appealing alternative to tackle this issue. Among these materials, copper is the most frequently used due to its efficiency in “contact killing” and therefore it has been used for multiple applications in the healthcare [6]. The mechanisms behind the antimicrobial activity of copper are not completely understood yet but it is commonly accepted that the release of ions from the surface plays an important role in this effect.

Most of the studies carried out over the years have focused on using copper and copper alloys in the crystalline state. The major drawbacks for using these materials are their relatively low hardness and low wear resistance. These properties can be increased when copper and copper alloys are in an amorphous (i.e., metallic glasses) or amorphous/crystalline state (i.e., metallic glass composites) [6]. This can be accomplished by increasing the glass forming ability (GFA) through alloying copper with other elements. However, addition of such elements may result in losing part of the antimicrobial ability when these elements are non-antimicrobial.

Metallic glasses exhibit higher yield strength and lower Young’s modulus than their crystalline counterparts resulting in higher wear resistance [7]. This has triggered a growing interest in designing novel copper-based metallic glasses [8] as touch surfaces. Despite the interest in the topic, the number of studies dealing with the antimicrobial behaviour of bulk metallic glasses (BMGs) is still very small. For example, Huang et al. [9] studied the antimicrobial effect against the Gram positive bacterium *S. aureus* of Cu-containing Zr-based BMGs. The authors concluded that the number of colony forming units (CFU) on Zr-based BMGs after 4 h of moist contact was about one order of magnitude lower than on Ti-6Al-4V alloy. From the point of view of the tribological behaviour of metallic glasses, there are numerous studies about the interaction of a cylindrical sample and a surface (pin-on disc) or the interaction between a diamond tip and the surface (scratch test) when the material is either in bulk shape or as thin film [7, 8, 10-13]. However, studies dealing with the ability to tune the wear resistance of metallic glasses by controlling the formation of intermetallic phases are scarce.

The aim of this study is to control the addition of Cu to metallic glass alloys corresponding to the Cu-Zr-Al system to promote the formation of Cu-rich intermetallic phases in order to optimize the mechanical and antimicrobial performance. These Cu-rich alloys are derived from a similar composition, $\text{Cu}_{50}\text{Zr}_{43}\text{Al}_7$ (at. %), with high GFA and strength [14]. The mechanical properties have been studied using nanoindentation and scratch studies. The antimicrobial studies have been performed using Gram-positive and Gram-negative bacteria since both types of bacteria can be found on touch surfaces and they exhibit different sensitivity against Cu ions [15]. Although some authors have previously studied the antimicrobial behaviour of Cu-containing metallic glasses [9, 16] the possibility of tuning the antimicrobial performance by controlling the formation of crystalline phase has been mostly overlooked.

2. Experimental

Alloy ingots with nominal composition $\text{Cu}_{50+x}(\text{Zr}_{44}\text{Al}_6)_{50-x}$ with $x=(0, 3 \text{ and } 6)$ were prepared from elements with purity higher than 99.9 at. %. The master alloys were re-melted three times in a Zr-gettered high

purity argon atmosphere to attain good chemical homogeneity. Rod samples of 2 mm in diameter were obtained from the master alloy by copper mould casting in an inert gas atmosphere. The structure of the as-cast and thermally-treated samples was studied by X-ray diffraction (XRD), using a Bruker D8 diffractometer with monochromated Cu K α radiation (2θ range 20°-90°, step size = 0.03°). The microstructure was investigated with a scanning electron microscope (SEM) (Mira FEM-SEM Tescan) equipped with energy-dispersive X-ray (EDX) analysis. To evaluate the mechanical properties, cylindrical specimens with 2:1 aspect ratio were tested at room temperature under compression at a strain rate of $2 \times 10^{-4} \text{ s}^{-1}$ in a universal Servosis machine. Nanoindentation experiments were performed at room temperature at approximately half the radius distance from the centre in a UMIS equipment from Fischer-Cripps Laboratories, in the load control mode and using a Berkovich-type diamond tip. Prior to the nanoindentation and scratch test the surfaces were mirror-like polished. The maximum load applied was 300 mN, high enough to make the indent deforming volume large enough to sample all the existing phases. A Teer Coating Limited scratch tester model ST220 was used for the scratch tests of the mirror-like polished samples. The tests were performed at a load of 30 N at a stage speed of 10 mm/min. The scratched surfaces (profile and roughness) were analysed using an Alicona profilometer and the profiles were obtained averaging 5 measurements. Contact angle measurements were carried out using the sessile drop technique, with a Krüss drop size DSA30 analyser and depositing 1 μl of deionized water at a rate of 30 $\mu\text{m}/\text{min}$.

For initial antimicrobial tests, *E. coli* strain K12 (Gram-negative) and *Bacillus subtilis* strain 168 (Gram-positive) were incubated (30°C), with shaking (200 rpm), in 25 ml of Mueller-Hinton Broth (MHB) for 16 hours. Cultures were diluted in MHB to an optical density (OD₆₀₀) of 0.01. The diluted cultures were incubated at 37°C until they reached an OD₆₀₀ of ~ 0.3. A quantity equal to 1 μl of the respective cultures was pipetted off directly onto the ground (4000 grit) surfaces of the specimen and control (copper and plastic) samples. Inoculated samples were placed inside a petri dish containing moist tissue, sealed and statically incubated for 4 hours at 37°C, after which they were diluted in 99 μl of MHB. Samples were serially diluted, plated onto MH agar and resulting colonies were counted after 16 hours of incubation at 37°C. All tests were done in triplicate and mean counts reported. Time-kill experiments were done as above, but a lower initial inoculum density was used (ca. 1×10^6 cells/ml) and cell counts were taken every hour 60 mins.

3. Results and discussion

3.1. Microstructure

Fig. 1 shows the XRD scans of 2 mm diameter rods of $\text{Cu}_{50+x}(\text{Zr}_{44}\text{Al}_6)_{50-x}$ ($x=0$, $x=3$ and $x=6$). For the $\text{Cu}_{50}\text{Zr}_{44}\text{Al}_6$ alloy high intensity peaks associated to orthorhombic $\text{Cu}_{10}\text{Zr}_7$ ($a = 0.9347 \text{ nm}$, $b = 0.9347 \text{ nm}$, $c = 1.2675 \text{ nm}$), orthorhombic Cu_8Zr_3 ($a = 0.78686 \text{ nm}$, $b = 0.81467 \text{ nm}$, $c = 0.9977 \text{ nm}$), B19' CuZr martensite and also probably austenite B2 CuZr are detected and superimposed on a broad halo suggesting that along with the crystalline phases an amorphous phase is present. For the $\text{Cu}_{53}\text{Zr}_{41.4}\text{Al}_{5.6}$ alloy, the intensity of the broad halo decreases while the intensity of the XRD peaks, especially those

detected at around 40°, increase. A larger number of peaks associated to $\text{Cu}_{10}\text{Zr}_7$ and Cu_8Zr_3 are also observed. Finally, for the alloy with highest content Cu content (i.e., $\text{Cu}_{56}\text{Zr}_{38.7}\text{Al}_{5.3}$), the broad halo is practically undetectable and the peaks corresponding to $\text{Cu}_{10}\text{Zr}_7$ and Cu_8Zr_3 further increase in intensity, especially the one at about 41.5°. The peaks also tend to get narrower, suggesting growth of the crystallite size and additional peaks corresponding to CuZr phases, both austenite B2 and martensite B19', are detected. These results show that, in general, the number and intensity of the XRD peaks tend to increase and the intensity of the broad halo to decrease with increasing Cu content thus suggesting a decrease in the glass forming ability (GFA). The detection of these phases is consistent with previous works on other ZrCu-based BMG composites [17-19]. The formation of the stable intermetallic phases $\text{Cu}_{10}\text{Zr}_7$ [20], Cu_8Zr_3 and CuZr could be due to strong interaction of Cu and Zr atoms since the enthalpy of mixing (ΔH_{mix}) of Zr-Cu pair is -23 kJ/mol, stronger than the Cu-Al pair ($\Delta H_{\text{mix}} = -1$ kJ/mol) [21].

To better understand the differences between the three alloy compositions, the microstructures were also investigated by scanning electron microscopy. Fig. 2 shows the backscattered SEM images from the cross section of the 2 mm diameter rods of the three compositions, acquired at half the radius distance from the centre. For the $\text{Cu}_{50}\text{Zr}_{44}\text{Al}_6$ alloy (Fig. 2a), crystalline phases of different sizes are observed, from equiaxed nuclei of less than 1 μm to dendrites whose arms expand up to 5 μm . The brightness of the equiaxed particles and that of the dendrites is very similar and therefore could be attributed to the same crystalline phase at different stages of growth. This phase is slightly darker than the matrix. A small area of higher brightness surrounding some of the dendrites are also observed and would be attributed to another crystalline phase and therefore two intermetallic phases of different composition seem to coexist together, in agreement with the XRD results. According to XRD, in principle, up to four intermetallics may be present in the $\text{Cu}_{50}\text{Zr}_{44}\text{Al}_6$ alloy, but matching these results with those from electron microscopy suggests that the two peaks at about 40 and to 43° would be attributed to $\text{Cu}_{10}\text{Zr}_7$, the peak at about 66° to martensite CuZr and the peak close to 37° to both phases ($\text{Cu}_{10}\text{Zr}_7$ and CuZr). The matching has been done taking into consideration the differences in atomic weight of the elements (Cu: 63.546, Zr:91.224 and Al:26.9815) [22] where a brighter backscattered image indicates a higher concentration of high atomic weight elements. The order from brightest to darkest is thus: Zr_1/Cu_1 (Cu_1Zr_1) > $\text{Zr}_7/\text{Cu}_{10}$ ($\text{Cu}_{10}\text{Zr}_7$) > Zr_3/Cu_8 (Cu_8Zr_3).

Bearing in mind the atomic weight of the constituent elements these round-shaped particles and the dendrites would correspond to $\text{Cu}_{10}\text{Zr}_7$ while the small brightest phase surrounding some dendrites to CuZr. For the alloy $\text{Cu}_{53}\text{Zr}_{41.4}\text{Al}_{5.6}$ (Fig. 2b) the microstructure changes dramatically since most of the crystalline phases consist of large and well-developed dendrites with arms of up to 10 μm length. However, small round crystalline phases of about 1 μm homogeneously dispersed in the matrix and also located around the dendrites are also present. This round phase is of similar brightness to that previously associated to $\text{Cu}_{10}\text{Zr}_7$ (Fig. 2a) and therefore should correspond to the same intermetallic phase. The dendrites correspond to the darkest phase and therefore should be associated to the phase with highest Cu content and would correspond to Cu_8Zr_3 . Not only the size of the dendrites have grown upon Cu addition, due to the decrease of the GFA, but also the surrounding clear phase associated to CuZr has

grown, suggesting that it has heterogeneously grown from the surface of the dendrites. Similar phenomena can be observed during the crystallization process in different alloy compositions where one crystalline phase grows from the previously formed phase [23]. The alloy with highest content copper, $\text{Cu}_{56}\text{Zr}_{38.7}\text{Al}_{5.3}$ (Fig. 2c) exhibits, at the half radius distance from the centre, a very similar microstructure to that of the alloy with 53 at. % Cu but the dendrites are more evolved. This confirms the decrease of the GFA with increasing Cu content. For this composition, and contrary to the alloys with 50 and 53 at. % Cu, no featureless matrix is observed and therefore it appears to be fully crystalline. The same three distinctive phases of different brightness are observed in this sample as well: dark dendrites (Cu_8Zr_3), a gray round phase ($\text{Cu}_{10}\text{Zr}_7$) and a matrix of lighter brightness (CuZr). These results are similar to those obtained by Yokoyama et al. [24] for alloys corresponding to the ZrCuAl system.

3.2. Mechanical behaviour

The mechanical behaviour of the alloys with 50, 53 and 56 at. % Cu were initially evaluated from compression tests. All the compositions were found to be brittle (i.e., the samples fractured in the elastic region) and therefore probably failed before the yield stress was reached (data not shown). Multiple step drops were detected in the elastic region upon loading, indicating the presence of internal flaws, probably porosity. This suggests that uniaxial compression is not a good technique to measure certain mechanical properties of these materials and therefore a more local technique where small sample volumes are involved in the deformation, was required. Nanoindentation is an excellent technique in such circumstances [25]. Furthermore, the wear resistance was assessed using scratch testing to compare the performance of the different alloys.

3.2.1. Nanoindentation tests

The mechanical behaviour of the three different investigated compositions was characterized by nanoindentation with a maximum load of 300 mN, large enough to sample all the crystalline phases and get average values of the different mechanical properties. Fig. 3 shows representative load-displacement (P-h) curves obtained at half the radius of the disk's cross-section. The maximum displacement h_{max} decreases with increasing the Cu content from $h_{\text{max}}=1.485 \mu\text{m}$ for $\text{Cu}_{50}\text{Zr}_{44}\text{Al}_6$ to $1.372 \mu\text{m}$ for $\text{Cu}_{56}\text{Zr}_{38.7}\text{Al}_{5.3}$. This can be ascribed to the increasing volume fraction of brittle and mechanically hard intermetallic phases. Remarkably, clear pop-in events are observed for the samples containing an amorphous fraction (i.e., 50 at.% and 53 at.% Cu) (see inset), which are indicative of shear band activity governing the deformation behaviour of these materials [26, 27].

Table 1 lists the values of the parameters H , E_r , H/E_r , H^3/E_r^2 and h_{max} for the studied alloys. The hardness increases from 8.46 GPa for $\text{Cu}_{50}\text{Zr}_{44}\text{Al}_6$ to 10.15 GPa for $\text{Cu}_{56}\text{Zr}_{38.7}\text{Al}_{5.3}$ alloy while for the intermediate composition (i.e., $\text{Cu}_{53}\text{Zr}_{41.4}\text{Al}_{5.6}$) the hardness is 9.37 GPa, closer to $\text{Cu}_{56}\text{Zr}_{38.7}\text{Al}_{5.3}$ than to $\text{Cu}_{50}\text{Zr}_{44}\text{Al}_6$. These results are consistent with the XRD scans (Fig. 1) since the degree of crystallinity for $\text{Cu}_{56}\text{Zr}_{38.7}\text{Al}_{5.3}$ and $\text{Cu}_{53}\text{Zr}_{41.4}\text{Al}_{5.6}$ alloys is closer to each other than from $\text{Cu}_{50}\text{Zr}_{44}\text{Al}_6$ alloy. The hardness is larger than those reported for Zr-based metallic glasses [28, 29] and ZrCu-based metallic glasses [30]. The increase

of hardness H with the Cu content is presumably associated to the brittle and hard $\text{Cu}_{10}\text{Zr}_7$, Cu_8Zr_3 intermetallic phases in $\text{Cu}_{50}\text{Zr}_{44}\text{Al}_6$ since for $\text{Cu}_{50}\text{Zr}_{50}$ the hardness at 300 mN (using the same experimental setup) was reported to be of only about 6 GPa [31].

The values of maximum displacement also agree with the hardness trend since an increase in hardness involves a lower ability to plastic deformation. Another important listed parameter is the contact modulus E_r , which gives information about the stiffness of the contact between the sample and the indenter tip. The values increase from 108 to 123 GPa as the content of Cu increases from 50 to 56 at. %. For the intermediate composition, the value of E_r (i.e., 121 GPa) is closer to that of $\text{Cu}_{56}\text{Zr}_{38.7}\text{Al}_{5.3}$ than to $\text{Cu}_{50}\text{Zr}_{44}\text{Al}_6$, which agrees with the relatively large fraction of crystalline phases in both samples. Nonetheless, this behaviour could also be attributed, at least in part, to differences in the composition since the Young's modulus of Cu (i.e., $E_{\text{Cu}}=130$ GPa), is higher than that of Zr and Al ($E_{\text{Zr}}=68$ GPa, $E_{\text{Al}}=70$ GPa) [32]. The value of E_r for $\text{Cu}_{50}\text{Zr}_{44}\text{Al}_6$ is not far from 112.5 GPa, previously reported for an alloy with similar composition [30]. These materials could also potentially exhibit good tribological performance, given their high H values and the bright appearance obtained after polishing their surfaces. In order to estimate the wear resistance, the values of H/E_r [33] and H^3/E_r^2 [34] were assessed since these parameters have been reported to be more representative of the wear resistance than the hardness itself. The parameter H/E_r^2 indicates the resistance to plastic deformation [35] and its dependence with the Cu content correlates well with that of the displacement values h_{max} from nanoindentation tests. The values of both H/E_r^2 and H^3/E_r^2 increase with increasing the Cu content. H/E_r^2 increases from 0.078 to 0.082, for $\text{Cu}_{50}\text{Zr}_{44}\text{Al}_6$ and $\text{Cu}_{56}\text{Zr}_{38.7}\text{Al}_{5.3}$ alloys, respectively, while H^3/E_r^2 increases from 0.052 to 0.069. These results suggest that the wear resistance of $\text{Cu}_{50+x}(\text{Zr}_{44}\text{Al}_6)_{50-x}$ alloys should be maximum for the most crystalline composition, i.e., $\text{Cu}_{56}\text{Zr}_{38.7}\text{Al}_{5.3}$. Hence, this behaviour can be associated with the nature and volume fraction of the crystalline phases in each composition. For further assessment of the wear resistance, scratch tests were also performed.

3.2.2. Scratch tests

In order to assess the wear behaviour of the different compositions scratch tests were performed at approximately half the radius distance from the centre. It is important to take into consideration that in scratch tests the deformation is more complex than in indentation since the material is not only subjected to a compressive load normal to the surface but simultaneously a shear load is acting parallel to the scratch direction. Differences in wear behaviour among the three compositions were analysed from the morphology of the scratches and the cross section profile as shown in Fig. 4. For each composition the pile-up size, groove depth at the centre and the maximum depth, the average (R_a) and total roughness (R_z) are indicated in the figure. Fig. 4a shows that the scratch for $\text{Cu}_{50}\text{Zr}_{44}\text{Al}_6$ alloy contains multiple lateral cracks in the pile-up separated at a distance of about 25 to 50 μm from each other. The cracks are relatively short (up to about 50 μm) and do not seem to propagate beyond the pile-up width. For the $\text{Cu}_{53}\text{Zr}_{41.4}\text{Al}_{5.6}$ alloy (Fig. 4b) the density of cracks growing from the scratch is much smaller and the distance from each other is larger. In addition, they are not confined to the pile-up but propagate larger

distances, up to 150 μm . The largest cracks are detected for the composition $\text{Cu}_{56}\text{Zr}_{38.7}\text{Al}_{5.3}$ alloy since they extend well beyond 200 μm and the crack density is also larger than for $\text{Cu}_{53}\text{Zr}_{41.4}\text{Al}_{5.6}$ alloy. Finally, for the composition $\text{Cu}_{56}\text{Zr}_{38.7}\text{Al}_{5.3}$ (Fig. 4c) the cracks are not only longer (they extend well beyond 200 μm) but their density is also higher (distance from each other from about 50 to 100 μm). Moreover, the cracks also propagate towards the inner part of the track as shown in the detail (red square). This feature is similar to the brittle tensile cracking observed by Bull [36] and therefore the results suggest that the composition $\text{Cu}_{56}\text{Zr}_{38.7}\text{Al}_{5.3}$ is very brittle. From crack analysis it can be clearly observed that the samples embrittle as the Cu content increases.

For each composition, along with the microscopy images, the 2D cross sectional profiles are shown (left panels). The horizontal red line corresponds to the substrate level and it is used as reference to measure the pile-up height (maximum) and groove depth, i.e., the depth of the track at the centre and maximum depth of the track. All these values have been obtained from 5 different measurements at about half the radius distance from the centre. For the $\text{Cu}_{50}\text{Zr}_{44}\text{Al}_6$ alloy the height of the pile-up is 4.13 ± 1.98 μm while the depth of the groove at the centre and at the maximum depth are 14.08 ± 1.20 and 22.20 ± 3.95 , respectively. However, as the alloy becomes richer in Cu ($\text{Cu}_{53}\text{Zr}_{41.4}\text{Al}_{5.6}$ composition in Fig. 4b), the height of the pile-up gets smaller and the groove depth at the centre and at the maximum depth increase slightly. The maximum height of the pile-up is only about 2.65 ± 1.71 μm while the depth at the centre and maximum depth reach 20.10 ± 7.1 μm and 31.1 ± 7.08 μm , respectively.

For the alloy with the highest content, $\text{Cu}_{56}\text{Zr}_{38.7}\text{Al}_{5.3}$ (Fig. 4c), the height of the pile-up decreases slightly to 2.10 ± 0.84 μm while the groove depth at the centre (20.00 ± 2.02 μm) and maximum depth (31.42 ± 5.56 μm) are very similar to those observed in $\text{Cu}_{53}\text{Zr}_{41.4}\text{Al}_{5.6}$ alloy. Differences can be also analyzed in terms of scratch groove volume to pile-up volume for the three compositions. The values are 5-6 for $\text{Cu}_{50}\text{Zr}_{44}\text{Al}_6$, 15-16 for $\text{Cu}_{53}\text{Zr}_{41.4}\text{Al}_{5.6}$ and 40-41 for $\text{Cu}_{56}\text{Zr}_{38.7}\text{Al}_{5.3}$. These results are consistent with the trend from XRD scans (Fig. 1) and SEM results (Fig. 3), since a small copper increase from 50 to 53 at. % changes the microstructure dramatically while from 53 to 56 at. % Cu microstructural differences are relatively small. However, the pile-up height and groove depth difference for the alloys with highest content of copper are negligible since they are within the error tolerance. The roughness of the groove surface at the track is significant and differences for the three compositions have been analyzed. Fig. 4b and 4c show that the profile is more abrupt than in Fig. 4a due to the local presence of narrow deep pits and suggests that alloys containing 53 and 56 at. % Cu are more prone to adhesive wear upon dry sliding. The last two compositions not only exhibit higher maximum depth than that of $\text{Cu}_{50}\text{Zr}_{44}\text{Al}_6$ alloy but also, the difference of distance between the maximum depth and the depth at the centre is ~ 11 μm versus ~ 8 μm for $\text{Cu}_{50}\text{Zr}_{44}\text{Al}_6$, suggesting that the groove is steeper due to the abrasion generated when the intermetallic particles are dragged. In any case, the profiles for the different compositions show common features, i.e., the groove depth at the centre of the track is generally smaller than at both sides probably because the brittle intermetallic particles (abrasive debris) pulled out by the tip tend to slide to both sides of the tip upon scratching and they are afterwards dragged along the track.

To better assess differences of wear mechanism among the three compositions, the morphological features from the track surface have been analyzed in detail (see magnified SEM images of Fig. 5). For each composition representative 2D cross sectional profiles obtained along the track centreline for a distance of 100 μm are also shown, but SEM images were taken from a smaller and representative distance. The alloy containing 50 at. % Cu (Fig. 5a) exhibits a relatively smooth smeared groove surface without signs of abrasion and consisting of a wavy profile (see inset) with roughness features ranging from a maximum height of 2 μm to a minimum depth of -1 μm . These features suggest ductile plowing and plasticity [37]. As the composition gets richer in Cu, the groove surface tends to turn rougher. For the composition $\text{Cu}_{53}\text{Zr}_{41.4}\text{Al}_{5.6}$ (Figs 5b) clear signs of significant detachment outlined by a sharp contour (chipping) (see small arrows) is observed, suggesting that adhesive transfer to the diamond tip has taken place. Small pits of about 1 μm size are also detected (wider arrow) which could be associated to the pulling out of the intermetallic particles due to adhesion of these particles to the diamond tip upon scratching. These results suggest that the particle-matrix interface is relatively weak. While the dendritic particles exhibit a rough enough contour to remain mechanically attached to the matrix, those particles that exhibit rather rounded shapes can slide and be pulled out more easily.

The cross sectional profile (inset of Figs 5b) exhibits a more rough pattern with grooves that tend to be deeper than for $\text{Cu}_{50}\text{Zr}_{44}\text{Al}_6$ alloy (for the representative profile of Fig. 5b the groove can be as deep as 3 μm). The large area of transferred particles are smeared across the surface as they are dragged forward by the scratch diamond leading to some surface roughening and adhesive wear. The smaller intermetallic particles are harder and generate abrasive damage as they slide across the surface.

For $\text{Cu}_{56}\text{Zr}_{38.7}\text{Al}_{5.3}$ alloy (Figs 5c) signs of detachment (small arrow) and pits (large arrow) are also detected observed but the volume fraction of pits is larger and the surface is more grooved than for the $\text{Cu}_{53}\text{Zr}_{41.4}\text{Al}_{5.6}$ alloy, which is consistent with the presence of a larger volume fraction of brittle crystalline phases. Additionally, microcracks are observed across the track. There is also evidence for smearing of material along the sample surface in the track. These features suggest that the material has been subjected to adhesive wear, although abrasive wear also takes place as deduced from the grooved surface similarly to that observed in Zr-based BMGs [38].

The roughness of the profile becomes even more prominent with maximum groove depth up to about 7 μm (see inset). Comparing the amplitude and spacing of the serrations one can observe that they tend to increase with increasing copper content.

It is interesting to observe that the depth of the grooves shown in Fig. 4 is larger for the alloys which are more brittle (highest Cu content). A priori, one might expect that the wear resistance should be higher in the mechanically harder alloys (i.e., Cu-rich), where the track depth should thus be smaller. This is opposite to our observations. This inconsistency with the hardness results (Table 1) can be attributed to the differences in the stress conditions of the material upon indentation and scratching (compression and shear forces). Namely, scratching is more sensitive to the properties of the matrix and the amount (and size) of precipitates, since a softer matrix would easily allow easier dragging of the precipitate particles. For $\text{Cu}_{56}\text{Zr}_{38.7}\text{Al}_{5.3}$ the size of the crystalline particles (dendrites and rounded particles) is larger, they are

very abundant and detach more easily from the matrix than for the alloys depleted in Cu and the precipitate particles tend to detach more easily in this case, causing larger grooves.

3.3 Wettability and Antimicrobial tests

To assess the potential interest of these alloys for antimicrobial applications not only antimicrobial tests were performed but also the wettability was studied since this provides useful information about the ability for bacterial adhesion on surfaces [39]. The wettability can be analysed by measuring the contact angle of sessile droplets. Fig. 6 shows the average water contact angle on the three alloys: 101.8° for Cu₅₀Zr₄₄Al₆, (Fig. 6 a), 99.8° for Cu₅₃Zr_{41.4}Al_{5.6}, (Fig. 6 b) and 90.2° for Cu₅₆Zr_{38.7}Al_{5.3} (Fig. 6 c). The angle 101.8° is not far from 106.6° detected in a fully amorphous Cu₄₈Zr₄₂Ti₄Al₆ at. % metallic glass thin film [40]. The decrease of the contact angle suggests that the material becomes more hydrophilic with increasing Cu content and therefore this should favour the adhesion of bacteria on the surface. This large effect is probably mostly associated with a change in the crystallinity rather than compositional change since similar differences in contact angle are reported when comparing Zr-based and Cu-based metallic glasses [40], i.e., alloys with very different compositions. However, the differences in Cu-content for the Cu-Zr-Al alloys studied here is of only 6 at. %.

The antimicrobial behaviour of the alloys was assessed from reduction in bacterial cells over the time for different initial bacterial densities. When 2.4×10^8 bacterial cells were applied to the surface of the samples, there was no reduction observed with sample Cu₅₀Zr₄₄Al₆ when compared to the control samples. After 4 hours of contact with the Cu₅₃Zr_{41.4}Al_{5.6} sample, *E. coli* and *B. subtilis* numbers were reduced by ca. 50% and 70% respectively. The Cu₅₆Zr_{38.7}Al_{5.3} sample reduced cell numbers by $\geq 90\%$ for both species (results not shown). For initial inoculum density of ca. 1×10^6 cells/ml, the time-kill curves were obtained for Cu₅₃Zr_{41.4}Al_{5.6} and Cu₅₆Zr_{38.7}Al_{5.3} samples up to 250 min (Fig. 7). Both alloys displayed a $> 3\text{-log}_{10}$ reduction in colony-forming units (cfu)/ml which is consistent with a bactericidal mode of action and with studies investigating bacterial surface contact with copper containing materials [41, 42]. In this study, *E. coli* was less resistant to contact killing than *B. subtilis*. This observation agrees with mode-of-action studies for copper-mediated killing of *E. coli* and *B. subtilis*, as *B. subtilis* produces endospores that are resistant to copper alloy surface killing [43]. The antimicrobial mode of action of copper is described as being reliant on three key properties: 1) copper oxidizes in air of moderate humidity, 2) the copper oxides formed are soluble in the aqueous phase, and 3) the copper ions are toxic to bacteria resulting in damage of intracellular components [44]. The antimicrobial properties of the samples investigated in this study are explained by their differing microstructures: the samples become more crystalline as the copper content increases, which should favour the release of Cu⁺ and Cu⁺⁺ cations through easier diffusion paths in crystalline than in amorphous structures. Furthermore, as the copper content increases, the samples become less hydrophobic and therefore the bacteria-surface contact area increases resulting in an improved rate of killing (Fig. 7). The findings in this study suggest that increasing the antimicrobial properties of copper metallic glass composites can be achieved by manipulating the microstructure of the

alloy through composition control. Among the three compositions studied, maximum antimicrobial behaviour and wear resistance is attained by the $\text{Cu}_{56}\text{Zr}_{38.7}\text{Al}_{5.3}$ composition and therefore it could be potentially interesting for the healthcare sector for which optimum performance is desired.

4. Conclusions

In this study, the antimicrobial activity and tribological behaviour of Cu-based BMG composites were investigated. The presence of an increasing content of hard intermetallic phases in the $\text{Cu}_{53}\text{Zr}_{41.4}\text{Al}_{5.6}$ and $\text{Cu}_{56}\text{Zr}_{38.7}\text{Al}_{5.3}$ alloys results in an increasing embrittlement of the $\text{Cu}_{50}\text{Zr}_{44}\text{Al}_6$ alloy. This is suggested by the cracks, lower pile-up, prone adhesion wear in dry sliding and higher scratch groove volume to pile-up volume revealed in the scratch test. The wear resistance also increases with increasing Cu content as indirectly assessed from H/E_r and H^3/E_r^2 parameters. The results from the sessile drop technique show lower contact angle values with increasing Cu content, which favours adhesion of bacteria to the substrate. The $\text{Cu}_{56}\text{Zr}_{38.7}\text{Al}_{5.3}$ alloy shows improved increase in contact killing for *B. Subtilis* and *E. Coli* during the first hour of interaction, which can be useful to prevent bacteria spreading on touch surfaces.

5. Acknowledgments

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Figures captions

Fig. 1. XRD scans for samples (a) $\text{Cu}_{50}\text{Zr}_{44}\text{Al}_6$ (b) $\text{Cu}_{53}\text{Zr}_{41.4}\text{Al}_{5.6}$ and (c) $\text{Cu}_{56}\text{Zr}_{38.7}\text{Al}_{5.3}$ alloys.

Fig. 2. Backscattered SEM images taken from the middle radius for a) $\text{Cu}_{50}\text{Zr}_{44}\text{Al}_6$ (b) $\text{Cu}_{53}\text{Zr}_{41.4}\text{Al}_{5.6}$ and (c) $\text{Cu}_{56}\text{Zr}_{38.7}\text{Al}_{5.3}$ alloys.

Fig. 3. Load-displacement (P-h) nanoindentation curves for a) $\text{Cu}_{50}\text{Zr}_{44}\text{Al}_6$ (b) $\text{Cu}_{53}\text{Zr}_{41.4}\text{Al}_{5.6}$ and (c) $\text{Cu}_{56}\text{Zr}_{38.7}\text{Al}_{5.3}$ alloys.

Table 1. Summary of the mechanical properties of the $\text{Cu}_{50}\text{Zr}_{44}\text{Al}_6$, $\text{Cu}_{53}\text{Zr}_{41.4}\text{Al}_{5.6}$ and $\text{Cu}_{56}\text{Zr}_{38.7}\text{Al}_{5.3}$ alloys after nanoindentation using a maximum load of 300 mN. The values of hardness (H), reduced Young's modulus (E_r), H/E_r , H^3/E_r^2 ratios and maximum indentation depth (h_{max}) are given in the table.

Fig. 4. Images showing the scratches at the middle radius of the samples a) $\text{Cu}_{50}\text{Zr}_{44}\text{Al}_6$ (b) $\text{Cu}_{53}\text{Zr}_{41.4}\text{Al}_{5.6}$ and (c) $\text{Cu}_{56}\text{Zr}_{38.7}\text{Al}_{5.3}$ alloys along with their corresponding 2D cross sectional profiles and numerical values.

Fig. 5. Images showing the central area of the scratches at the middle radius of the samples a) $\text{Cu}_{50}\text{Zr}_{44}\text{Al}_6$ (b) $\text{Cu}_{53}\text{Zr}_{41.4}\text{Al}_{5.6}$ and (c) $\text{Cu}_{56}\text{Zr}_{38.7}\text{Al}_{5.3}$ alloys along with their corresponding 2D cross sectional profiles and numerical values.

Fig. 6. Average water contact angle on Cu-Zr-Al alloys (a, b and c).

Fig. 7. Time-kill curve of *E. coli* K12 and *B. subtilis* 168 exposed to Cu-Zr-Al alloys for up to 250 min.

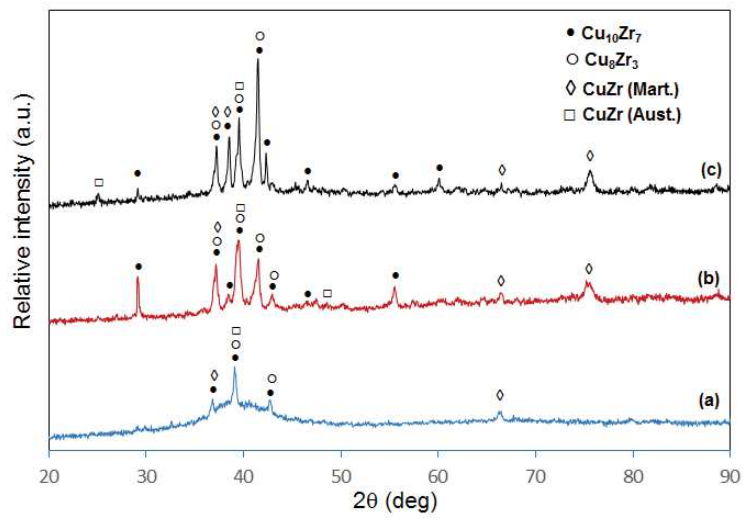


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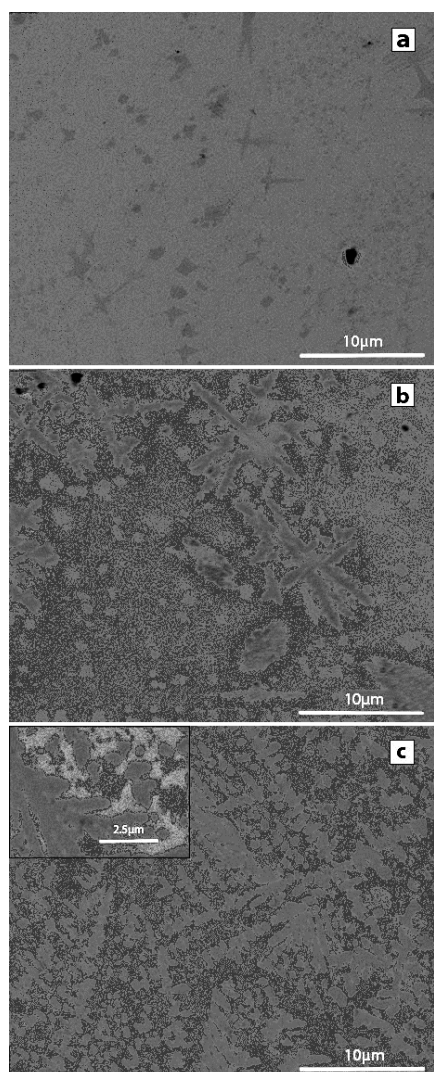


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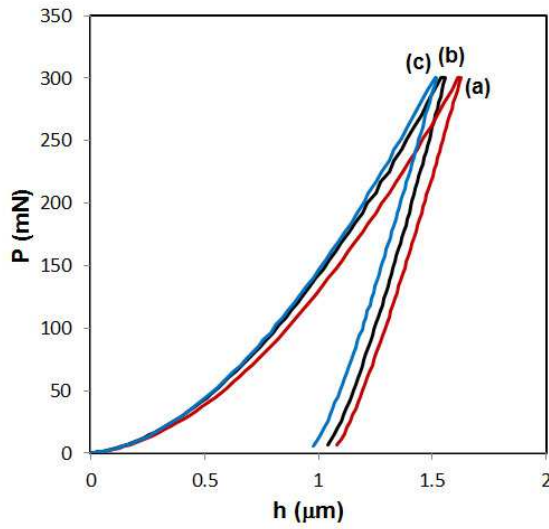


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Property	$\text{Cu}_{50}\text{Zr}_{44}\text{Al}_6$	$\text{Cu}_{53}\text{Zr}_{41.4}\text{Al}_{5.6}$	$\text{Cu}_{56}\text{Zr}_{38.7}\text{Al}_{5.3}$
$H(\text{GPa})$	8.46 ± 0.45	9.37 ± 0.28	10.15 ± 1.87
$E_r(\text{GPa})$	107.96 ± 3.57	121.19 ± 1.87	123.36 ± 6.89
H/E_r	0.078 ± 0.007	0.077 ± 0.003	0.082 ± 0.020
$H^3/E_r^2(\text{GPa})$	0.052 ± 0.006	0.056 ± 0.007	0.069 ± 0.046
$h_{\text{max}}(\mu\text{m})$	1.485 ± 0.035	1.403 ± 0.017	1.372 ± 0.081

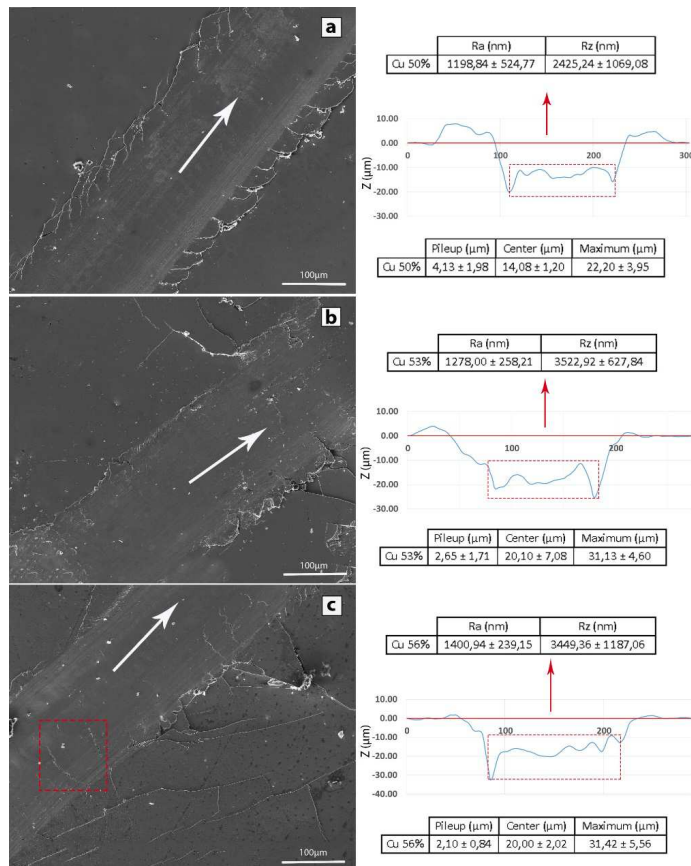


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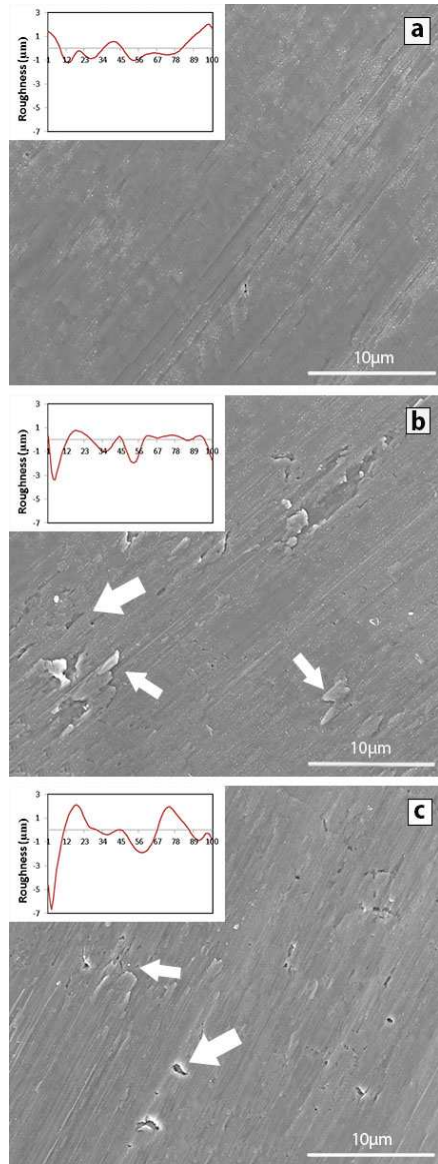


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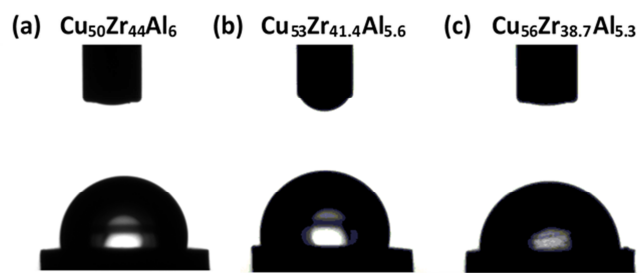


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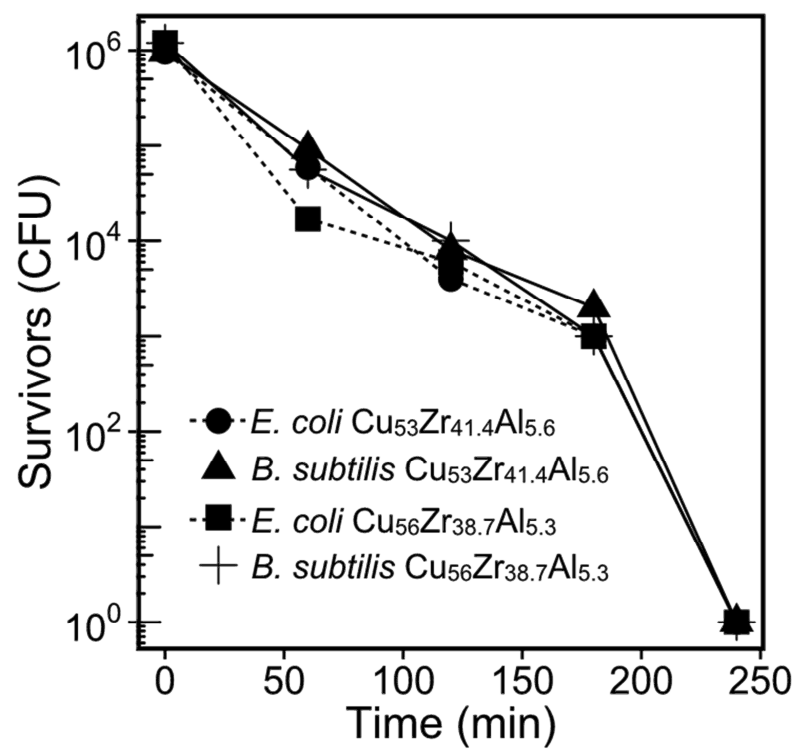


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