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# Production of biofunctionalized MoS<sub>2</sub> flakes with rationally modified lysozyme: a biocompatible 2D hybrid material

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**Keywords:** lysozyme, 2D materials, MoS<sub>2</sub>, biocompatibility, biofunctionalized material.

Supplementary material for this article is available online

## Abstract

Bioapplications of two-dimensional materials embrace demanding features in terms of environmental impact, toxicity and biocompatibility. Here we report on the use of a rationally modified lysozyme to assist the exfoliation of MoS<sub>2</sub> bulk crystals suspended in water through ultrasonic exfoliation. The design of the proposed lysozyme derivative provides this exfoliated 2D-material with both, hydrophobic groups that interact with the surface of MoS<sub>2</sub> and hydrophilic groups exposed to the aqueous medium, which hinders its re-aggregation. This approach, clarified also by molecular docking studies, leads to a stable material ( $\zeta$ -potential,  $27 \pm 1$  mV) with a yield of up to 430  $\mu\text{g/mL}$ . The bio-hybrid material was characterized in terms of number of layers and optical properties according to different slots separated by diverse centrifugal forces. Furthermore the obtained material was proved to be biocompatible using human normal keratinocytes and human cancer epithelial cells, whereas the method was demonstrated to be applicable to produce other 2D materials such as graphene. This approach is appealing for the advantageous production of high quality MoS<sub>2</sub> flakes and their application in biomedicine and biosensing. Moreover, this method can be applied to different starting materials, making the denatured lysozyme a promising bio-tool for surface functionalization of 2D materials.

## Introduction

Two dimensional (2D) materials possess outstanding properties that are opening the path to a wide range of unprecedented scientific and technological applications [1]. Among the emerging 2D materials, molybdenum disulphide ( $\text{MoS}_2$ ) is particularly interesting due to its potential applications in catalysis [2], opto/electronics [3, 4] and biomedicine [5, 6]. As a transitional metal dichalcogenide,  $\text{MoS}_2$  is a semiconductor with an indirect bandgap of about 1.2 eV in the bulk form [7–9]. Though, decreasing the thickness of this material, from the bulk to the monolayer, the band gap of  $\text{MoS}_2$  increases to 1.9 eV [10]. Moreover, it changes from indirect to direct band [2]. In addition, recent works report that  $\text{MoS}_2$  in the form of a few-layer or monolayer crystal is photoluminescent, which is attributed to the direct gap in the electronic structure of  $\text{MoS}_2$  [11–13]. Consequently, this novel material is appealing for innovative photovoltaic and photocatalytic applications [14–16] and the generation of  $\text{MoS}_2$  monolayers is a critical step for the development of novel devices based on this 2D material [17].

Single-layer  $\text{MoS}_2$  can be viewed as an “S–Mo–S” sandwich structure, in which a plane of molybdenum atoms is layered between two planes of sulphur atoms. Each Mo is coordinated to six S atoms according to a trigonal prismatic geometry. As the stacked S–Mo–S layers are bound by weak van der Waals interactions [18, 19], it is possible to generate individual  $\text{MoS}_2$  nano/micro sheets by exfoliation of bulk  $\text{MoS}_2$  crystals [20, 21].

Several approaches have been developed for the production of  $\text{MoS}_2$ . The simplest strategy is a micromechanical cleavage using the scotch-tape method [4, 22, 23]. This method leads to the production of high quality material but is not suitable for the large-scale production of  $\text{MoS}_2$  due to the low yield, and to the fact that the size and thickness of the resultant  $\text{MoS}_2$  micro/nanosheets are difficult to control. Chemical vapour deposition allows for the production of high quality  $\text{MoS}_2$  sheets with excellent yield, but the complex experimental requirements limit the wide applicability of the method [20, 24, 25]. Compared to the aforementioned methods, liquid-phase exfoliation provides large quantity of high quality flakes at low costs [26]. Typically, liquid-phase exfoliation involves the use of ultrasonication in organic solvents [27–29], such as N-methylpyrrolidone and dimethylformamide, or in water in the presence of suited surfactants [30, 31]. After their preparation, the micro/nanosheets can be easily sorted and separated [32], resulting in a desirable size and thickness, moreover, by changing the solvent or the surfactant it is possible to obtain materials with different properties and applications.

Biomedical applications of  $\text{MoS}_2$  involve major concerns such as environmental impact, toxicity and biocompatibility [6, 33]. The use of biomolecules, such as proteins, during the exfoliation leads to several advantages including a low environmental impact, biocompatibility of the resulting material, and easier functionalization of the flakes avoiding covalent modifications that could change the properties of the material. In fact, bioconjugation of  $\text{MoS}_2$  sheets is crucial for different applications

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3 in the biotechnological and biomedical fields (i.e. drug delivery, tissue engineering, biosensors,  
4 scaffolds, etc.) [21, 34]. During the last years, several approaches have been developed for the liquid-  
5 phase exfoliation of MoS<sub>2</sub> using biomolecules, such as polysaccharides [35–37], DNA/RNA  
6 nucleotides [34, 37], and proteins [38, 39].  
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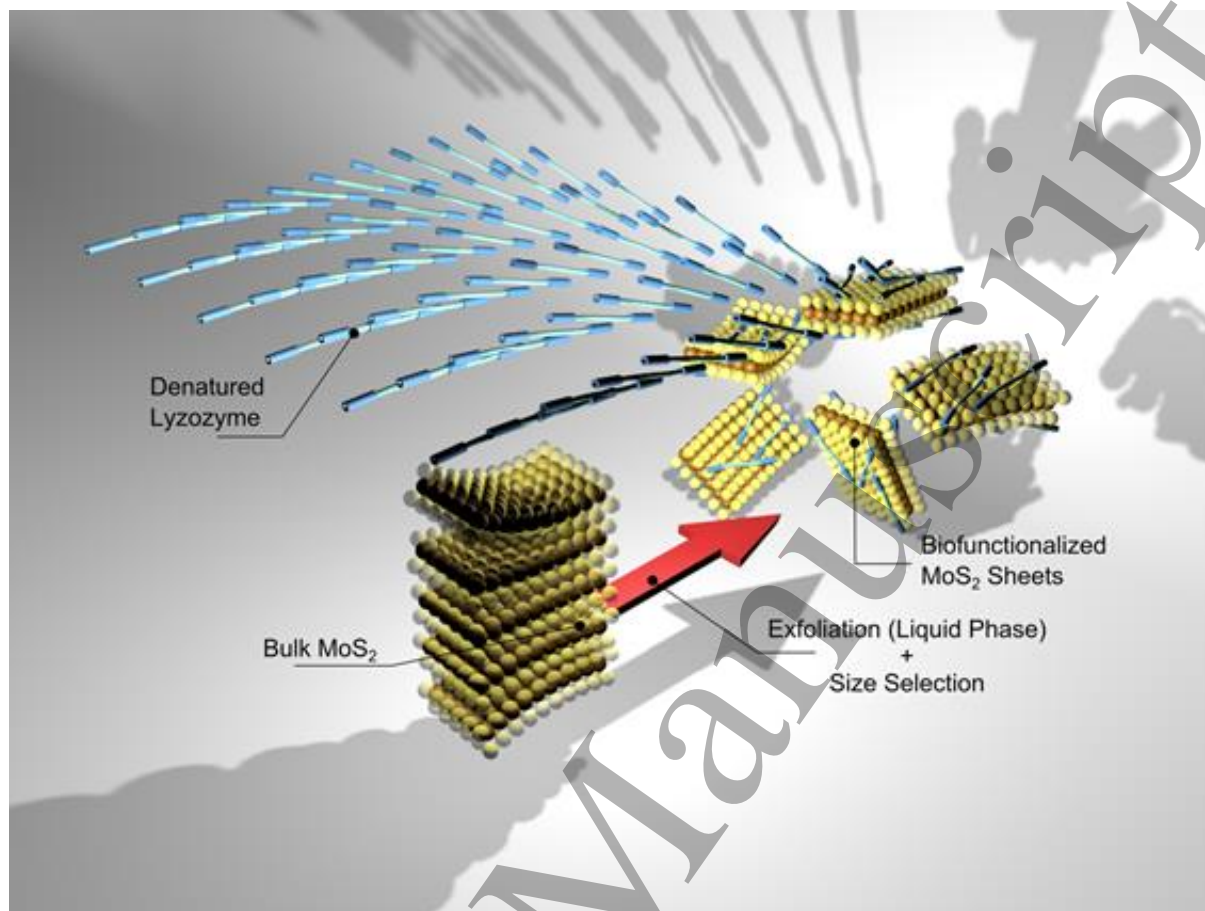
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10 Recently, Guan et al. reported the production of water soluble MoS<sub>2</sub> using bovine serum albumin  
11 (BSA) [39]. MoS<sub>2</sub> powder was sonicated during 48 h with BSA obtaining exfoliated / soluble material  
12 whose maximum concentration was 1.36 mg mL<sup>-1</sup>, with a production rate of 0.38 μg mL<sup>-1</sup> h<sup>-1</sup>.  
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15 More recently, Forsberg and co-worker reported a different approach to obtain MoS<sub>2</sub> in water, by  
16 combining mechanical and liquid exfoliation, and obtaining 0.14 mg mL<sup>-1</sup> of MoS<sub>2</sub> after 1 h  
17 sonication [41], a value lower than that obtained by Guan [39]. Ayan-Varela and colleagues reported  
18 the use of nucleotides to solubilize MoS<sub>2</sub>, obtaining a dispersion with a yield which was inversely  
19 related to nucleotide concentration, reaching a maximum of 5-10 mg mL<sup>-1</sup> (production rate of 1-2 mg  
20 mL<sup>-1</sup> h<sup>-1</sup>). However, the thickness of the flakes was inversely related to nucleotide concentration, with  
21 smaller and thinner flakes present at higher nucleotide concentration [34]. Thus, even if in the last few  
22 years important advances have been achieved in the field of the MoS<sub>2</sub> exfoliation with biomolecules,  
23 obtaining a biocompatible material still is not completely investigated. Furthermore, the development  
24 of fast and universal approach for the large-scale production of MoS<sub>2</sub>, also applied to different 2D  
25 materials, aiming to obtain materials endowed with unique properties, is still a challenge.  
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28 We believe that MoS<sub>2</sub> exfoliation in the liquid phase can be benefited by using a rationally modified  
29 protein endowed with specific amphiphilic properties that is with hydrophobic groups able to interact  
30 with the surface of MoS<sub>2</sub> and hydrophilic groups exposed to the aqueous medium which should  
31 stabilize the delaminated material and prevent its re-aggregation. Herein, we designed a denatured,  
32 stable and fully soluble lysozyme derivative bearing amino-propyl moieties bound to the eight  
33 cysteine residues (aminopropyl-lysozyme, AP-LYS) [42], which is able to promote the formation of  
34 highly stable protein-decorated MoS<sub>2</sub> flakes. We report the production of biofunctionalized MoS<sub>2</sub>  
35 using liquid-phase exfoliation via ultrasound waves in the presence of AP-LYS. As depicted in Figure  
36 1, the bulk form of the material was ultrasonicated in aqueous solution. Subsequently, AP-LYS,  
37 thanks to its amphiphilic region, is adsorbed onto the exfoliated MoS<sub>2</sub>, stabilizing and functionalizing  
38 the exfoliated material. Centrifugations at different centrifugal forces were performed to control and  
39 select flakes with different size, obtaining a highly stable material. Docking studies were also  
40 performed to propose a theoretical model of the interaction between the rationally modified protein  
41 and the exfoliated MoS<sub>2</sub>. The production optimization, biofunctionalization, number of layers,  
42 stability, optical properties, yield and potential biocompatibility were systematically studied and the  
43 applicability of the method to produce other 2D materials such as graphene was also confirmed.  
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46 This approach can be applied for a large scale production of MoS<sub>2</sub> increasing its biocompatibility and  
47 dispersibility for various applications. This method allows the utilization of low-cost precursors, such  
48 as a powder, avoiding the addition of organic solvent.  
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The bio-hybrid material is endowed of unique properties and applicability in biotechnological and biomedical field.



**Figure 1.** Schematic model of the MoS<sub>2</sub> exfoliation assisted by AP-LYS. MoS<sub>2</sub> is exfoliated via ultrasound waves in aqueous solution. AP-LYS, thanks to its amphipathic regions, adsorbs onto the surface of the material. Micro/nanosheets with different number of layer are selected by centrifuging at different centrifugal force.

## Methods

**Docking of lysozyme fragment 1-18.** The interaction of fragment 1-18 of lysozyme with the surface of a MoS<sub>2</sub> monolayer was modelled by using a Monte Carlo energy minimization strategy which has already proved useful for the modelling of several complexes between biological macromolecules and ligands of different nature and size [43–47]. All calculations were performed using the ZMM-MVM molecular modelling package (ZMM Software Inc. [http://www.zmmsoft.com]). ZMM software allows conformational searches using generalized coordinates (e.g. torsion and bond angles) instead of conventional Cartesian coordinates [48], thus making the conformational search faster and much more efficient than usually obtained with other methods. Atom-atom interactions were evaluated using the Amber force fields [49] with a cutoff distance of 8 Å. Conformational energy calculations

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3 included van der Waals, electrostatic, H bond, and torsion components. Electrostatic interactions were  
4 calculated using an environment- and distance-dependent dielectric permittivity according to a  
5 method implemented in the ZMM software. Energy calculations also included a hydration component  
6 calculated as previously described [49, 50]. The model included lysozyme fragment 1-18 and a MoS<sub>2</sub>  
7 monolayer.  
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10 The monolayer contained 1020 MoS<sub>2</sub> units arranged to form a square with a side of about 91Å. Partial  
11 charges assigned to Mo and S atoms were +0.22 and -0.11 [52]. The MoS<sub>2</sub> monolayer was frozen  
12 throughout the simulation process.  
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15 The sequence of the modelled lysozyme fragment was NH<sub>2</sub>-KVFGRCELAAAMKRHGLD-CONH<sub>2</sub>.  
16 We choose to model an amidated C-terminus in order not to insert a negative charge not present in the  
17 protein. Cysteine at position 6 was modelled as an aminopropyl-cysteine. Histidine at position 17 was  
18 modelled in the protonated form as all the exfoliation experiments were conducted at pH 5. Initial  
19 structures of the fragment were prepared using PyMOL (DeLano Scientific LLC,  
20 <https://www.pymol.org/>) and DeepView - Swiss-PdbViewer [53]. Two initial structures were  
21 modelled, a completely helical and a completely extended structure. Each structure was used to  
22 generate four starting manually prepared complexes: fragment 1-18 was placed parallel to the surface,  
23 along one of the diagonals of the MoS<sub>2</sub> monolayer, hence the peptide structure was rotated by steps of  
24 90°. Each of the eight models was used as starting point for a Monte Carlo trajectory. Trajectories  
25 were stopped when no energy decrease was observed for 1000 minimization cycles.  
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28 **Exfoliation Process.** Molybdenum disulphide powder (Aldrich, 234842), was shaken using a TS-100  
29 Thermo-Shaker (Biosan, Riga, Latvia) at 650 rpm over night at 4°C in batches of 5 mL of 10 mM  
30 Sodium Acetate pH 5 with 0.2-1 mg mL<sup>-1</sup> AP-LYS [42], and then sonicated with a medium power tip  
31 sonicator (Q125 Sonicator, QSonica, 125 W, 20 kHz, inbuilt power meter power output, 19 W) in an  
32 ice bath. The dispersion was centrifuged at different centrifugal force using a Sigma 1-15 Fisher  
33 Bioblock scientific centrifuge. The UV-Vis spectra of the supernatants were acquired using UV-vis  
34 spectrophotometer Cary 4000 Scan using a quartz cell 1 cm optics. Concentration of dispersion was  
35 estimated by UV-vis spectroscopy, using the linear relationship of the concentration and absorption  
36 intensity at 666 nm previously established by Guan et al [39].  
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39 Graphite powder (Aldrich, 332461) (2 mg mL<sup>-1</sup>) was exfoliated as previously described in the  
40 presence of AP-LYS (0.2 mg mL<sup>-1</sup>). After consecutive centrifugations at 40, 2500 and 4500 g, the  
41 concentration of dispersions were determined using the absorption coefficient value at 660 nm (1390  
42 g L cm<sup>-1</sup>), as previously reported [54].  
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45 **Characterization.** Photoluminescence has been performed using a Hitachi F-2500 spectrometer. The  
46 sample was excited at 342 nm. The emission spectra were recorded in the range 383-600 nm.  
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49 Scanning Electron Microscopy (SEM) were performed by dropping 3 µL of solution on silicon chip.  
50 Images were recorded using FEI Quanta 650 FEG ESEM, 2 kV microscope.  
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3 AFM measurements were performed on silicon chip using a Nanoscope V Multimode8 AFM (Bruker,  
4 Germany) and Si cantilevers (SNL model, k:0.3N/m, Bruker). The scanning probe microscopy was  
5 carried out at a scan rate of 1 Hz and  $512 \times 512$  pixel. The silicon chip was dipped in the solution and  
6 dried by evaporation at room temperature under a ventilated fume hood. Electrokinetic analysis and  $\zeta$ -  
7 potential were carried out in folded capillary cells using a Malvern Zetasizer Nano-ZS system  
8 equipped with a 633 nm He-Ne laser. All measurements were conducted at 25 °C. For the Raman  
9 spectroscopy, samples were dropped on corning microscope glass slides (Aldrich, CLS294775 $\times$ 25),  
10 laser was focused on samples and multiple spectra were accumulated. The spectra were recorded with  
11 Horiba JobinYvonLabRAM HR 800, 800 mm focal length, 100 $\times$  objective, excitation wavelength 532  
12 nm.

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19 **Biocompatibility.** 2000 HeLa cells and 5000 HaCaT cells were seeded in 96 well-plates as  
20 monolayer. After 24 hours, cells were incubated in the presence of increasing concentration of AP-  
21 LYS/MoS<sub>2</sub> sample (5-10-20-50-100  $\mu\text{g mL}^{-1}$ ) for 24-48 hours, in complete medium at 37 °C in a  
22 humidified atmosphere containing 5% CO<sub>2</sub>. At the end of incubation, AlamarBlue® reagent  
23 (Invitrogen) was added in each well and incubated for 3 h at 37°C. The fluorescence intensity was  
24 measured at an emission wavelength of 585 nm and an excitation wavelength of 570 nm using a plate  
25 reader (Synergy HTX Multi-Mode Reader-BIOTEK). Cell survival was expressed as the percentage  
26 of viable cells in the presence of the AP-LYS/MoS<sub>2</sub> sample compared to controls. Two groups of cells  
27 were used as control, i.e. untreated cells and cells supplemented with identical volumes of buffer.  
28 Each sample was tested in three independent analyses, each carried out in triplicate. Quantitative  
29 parameters were expressed as the mean value  $\pm$  SD. Significance was determined by Student's t-test at  
30 a significance level of 0.05.

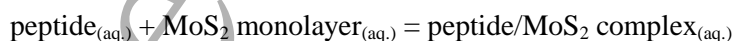
## 31 32 33 34 35 36 37 38 39 40 41 **Result and Discussion**

### 42 43 44 **Molecular docking analysis**

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46 As we have discussed previously, the ability of AP-LYS to promote the solubilisation of hydrophobic  
47 materials is likely related to the fact that the denaturation process significantly increases the molecular  
48 surface and the flexibility of lysozyme, and exposes to the solvent hydrophobic residues usually  
49 buried inside the hydrophobic core of the native protein [42]. However, even if AP-LYS is essentially  
50 unfolded in water, it is prone to regain a significant content of helical structure in the presence of  
51 trifluoroethanol [54–59], an organic solvent widely used to mimic the interaction of protein and  
52 peptide with detergent micelles and biological membranes. Very interestingly previous studies  
53 suggest that this increased content of helical structure is likely due to the refolding of the amphipathic  
54  $\alpha$ -helices located at the N- and C-terminus of the native lysozyme [61]. On the basis of these  
55 observations it can be hypothesized that the interaction of AP-LYS with 2D materials like MoS<sub>2</sub> and  
56 graphene is due to an adsorption process of amphipathic secondary elements of the denatured protein  
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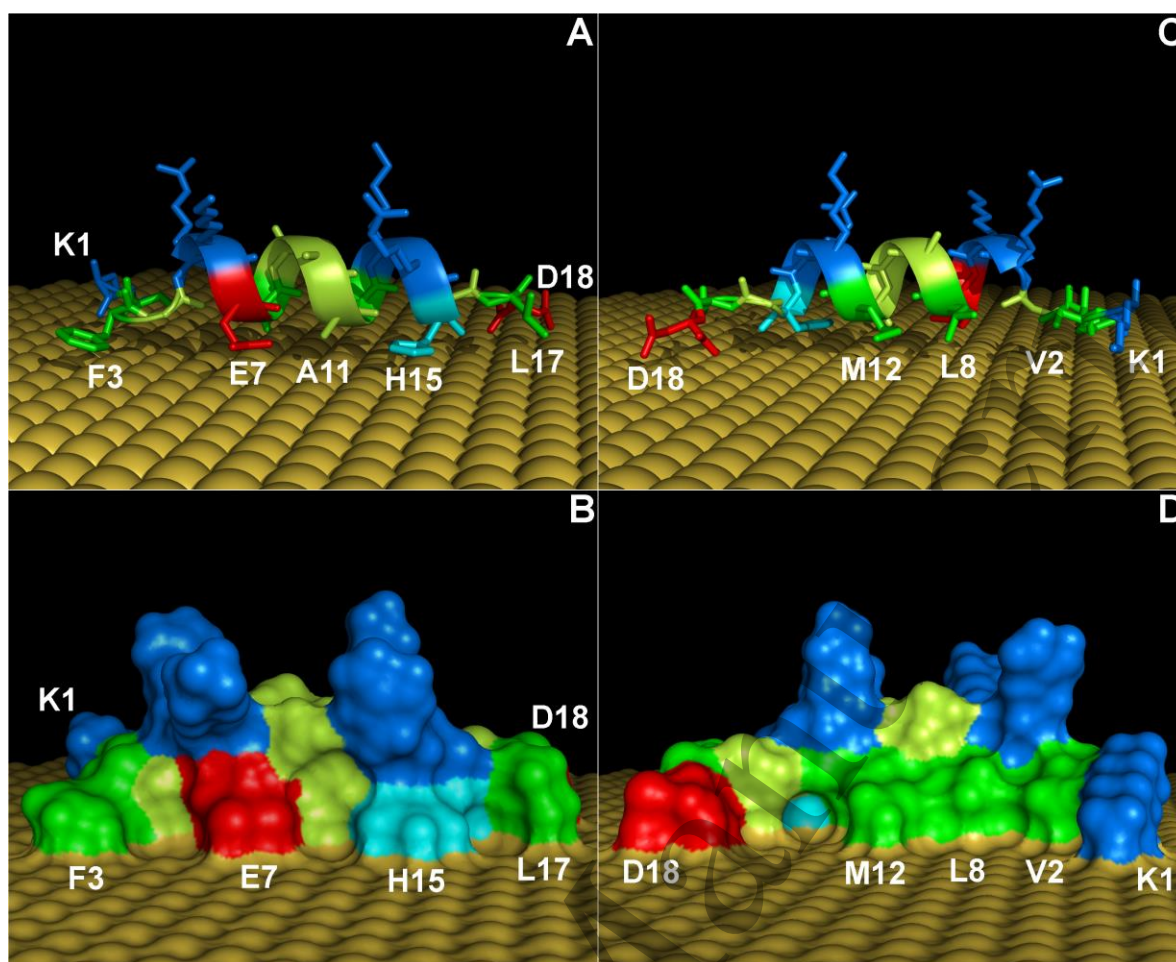
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3 onto the hydrophobic surface of these materials. The high positive charge of the hydrophilic sides  
4 would then stabilize the exfoliated material in water. In order to verify this hypothesis we modeled the  
5 interaction of residues 1-18 of lysozyme, which include the first amphipathic  $\alpha$ -helix (residues 4-15),  
6 with a  $\text{MoS}_2$  monolayer. The search for the lowest energy complex was performed by a Monte Carlo-  
7 based strategy starting from two limit structures – $\alpha$ -helix or extended– each placed in four different  
8 orientations above the  $\text{MoS}_2$  sheet (see Figure 2). In the lowest energy complex the lysozyme  
9 fragment adopts a structure which is intriguingly similar to that observed in the native protein. In fact,  
10 residues 5-15 form an amphipathic  $\alpha$ -helix with the hydrophobic residues Leu-8, Ala-11 and Met-12  
11 and two adjacent hydrophilic residues (Glu-7 and His-15) closely packed onto the surface. Residues  
12 1-4, which in the native protein are folded to pack the hydrophobic residues Val-2 and Phe-3 against  
13 the hydrophobic core in the complex, form a turn allowing these two residues to contact the surface of  
14 the  $\text{MoS}_2$  monolayer. Similarly residues 16-18 adopt a non-helical conformation allowing the binding  
15 of residues Leu-17 and Asp-18 to the surface. Table S1 shows the residues whose contribution to the  
16 binding energy is higher than 0.1 kcal/mol. Not surprisingly the highest contributions are from Phe-3  
17 and His-15 due to a stacking interaction between the rings in the side chains of these residues and the  
18 surface. These two residues also show the highest average contribution per sulphur atom on the  
19 surface. This result is due to the high polarizability of the pi systems in the side chains of  
20 phenylalanine and histidine which determines stronger van der Waals interactions. Interestingly three  
21 hydrophilic residues, Lys-1, Glu-7, and Asp-18, contribute significantly to the binding energy. In the  
22 case of Glu-7, the planar moiety  $-\text{CH}_2\text{-COO}^-$  lays parallel to the  $\text{MoS}_2$  surface. Similarly in the case of  
23 Lys-1, the terminal moiety  $-\text{CH}_2\text{-NH}_3^+$  lays close to the surface. In the case of Asp-18 both the main-  
24 chain and the side-chain make van der Waals interaction with the surface.

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40 We also modelled fragment 1-18 alone (Supp. Figure S1) in order to calculate a theoretical change in  
41 Gibbs free energy  $\Delta G$  for the adsorption reaction:



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46 The value we found, -5.3 kcal/mol (corresponding to a binding constant  $K = 1.7 \cdot 10^3$ ), suggests a  
47 relatively high affinity of fragment 1-18 for the  $\text{MoS}_2$  surface. Taking into account that AP-LYS  
48 contains six additional amphipathic secondary structure elements which could contribute  
49 cooperatively to the binding, it can be concluded that the docking analysis supports the hypothesis  
50 that adsorption of AP-LYS to the  $\text{MoS}_2$  surface is mediated by the binding of amphipathic regions of  
51 the denatured protein.  
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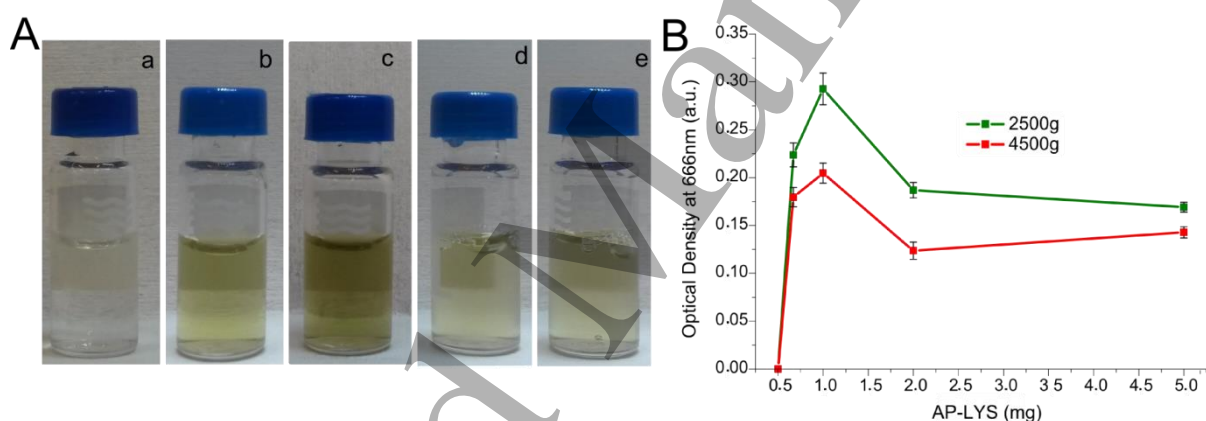


**Figure 2.** Docking of fragment 1-18 of hen egg lysozyme onto the surface of a MoS<sub>2</sub> monolayer. Residues are colored according to their properties: green, hydrophobic; light green, borderline residues (alanine, glycine); blue, positively charged; red, negatively charged; cyan, histidine. In panels A and C the protein fragment is shown as cartoon and sticks to highlight the secondary structure of the peptide and the side chains contacting the sulfur atoms of the surface (shown as dark yellow spheres). In panel C the structure is rotated by 180° around an axis perpendicular to the surface as compared to panel A. Panels B and D show the solvent accessible surface of the complex for the orientations shown in panels A and C, respectively. Labels are shown only for the residues making significant interaction with the surface (the corresponding binding energy values and the number of surface sulfur atoms involved in the interaction are shown in Table S1).

### Optimization process

In order to verify the effect of AP-LYS in the exfoliation of MoS<sub>2</sub> a fixed amount of MoS<sub>2</sub> powder (10 mg) was mixed with increasing amounts of AP-LYS (from 0.5 mg to 5 mg) in 5 mL of 10 mM sodium acetate pH 5. After shaking overnight, the suspensions were sonicated for 7 hours and subjected to centrifugation at increasing centrifugal forces (40 g, 2500 g and 4500 g). In the presence of the lowest amount of AP-LYS (0.5 mg, sample “a” in Figure 3A), the suspension appeared clear and colourless, whereas the rest of suspensions showed a yellow colour (samples from “b” to “e” in Figure 3A). Hence, the suspensions were analysed by UV/Vis spectroscopy to determine the amount of MoS<sub>2</sub> in solution. In Figure 3B the absorbance at 666 nm, which corresponds to the  $\lambda_{\max}$  of a MoS<sub>2</sub>

monolayer, is reported respectively as a function of the centrifugal force and amount of protein. In the presence of 0.5 mg of AP-LYS no MoS<sub>2</sub> was detectable in the solution. By increasing the amount of AP-LYS, from 0.5 mg to 1mg (Figure 3B and Figure S2), the concentration of MoS<sub>2</sub> in solution significantly increased, and the maximum yield was obtained in the presence of 1mg of AP-LYS. Increasing the amount of AP-LYS from 1 to 2 mg caused a decrease in the concentration of MoS<sub>2</sub> in solution but further increases (5 mg) caused no significant variation in the yield of soluble MoS<sub>2</sub> (Figure 3B). The saturation at high concentrations of AP-LYS can be tentatively explained assuming that the effect of AP-LYS requires its adsorption onto the surface of MoS<sub>2</sub> crystals, once the surface becomes saturated any further increase in the concentration of the protein will not increase the exfoliation efficiency. Although it is not particularly straightforward to find a detailed explanation for the higher exfoliation yields obtained using 1 mg of AP-LYS, a similar behaviour has been previously observed exfoliating either MoS<sub>2</sub> in the presence of (deoxy)ribonucleotides [34] and BSA [39] or WS<sub>2</sub> in the presence of seaweed alginate [37]. This suggests that the existence of an optimal concentration of additive is a general feature of biomolecule-mediated exfoliation of 2D materials.



**Figure 3.** Evaluation of AP-LYS concentration on the MoS<sub>2</sub> exfoliation. A) MoS<sub>2</sub> dispersions of obtained with a) 0.5 mg; b) 0.67 mg; c) 1 mg; d) 2 mg; e) 5 mg of AP-LYS. B) Normalized absorbance at 666nm reported as function of amount of AP-LYS used

In order to optimize the production of MoS<sub>2</sub>, different parameters were evaluated to achieve the best condition for the exfoliation: amount of starting material, MoS<sub>2</sub>/protein ratios, AP-LYS concentration and ionic strength (Figure S3A). All dispersions were sonicated (1h) and centrifuged (40g) in order to remove the non-exfoliated material. The amount of exfoliated material in suspension was determined spectrophotometrically (Figure S3C and E). The highest yields of exfoliated material were obtained using a protein: MoS<sub>2</sub> ratio = 1:10 (w/w) and 0.2 mg mL<sup>-1</sup> of MoS<sub>2</sub> in the presence of 10 mM NaAc pH 5.

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3 All the samples showed  $\zeta$ -potential values in the range +24 /+39 mV thus clearly indicating that the  
4 flakes of MoS<sub>2</sub> in suspension are covered by the cationic protein. The measured  $\zeta$  -potential values are  
5 generally associated to particles with a moderate to good stability in suspension (Figure S3B and D).  
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8 It is interesting to note that only in the case of the highest concentration of sodium acetate (30 mM)  
9 we obtained high standard deviations. These undesired variations among the replicates would suggest  
10 a reduced stability of the material at high ionic strength.  
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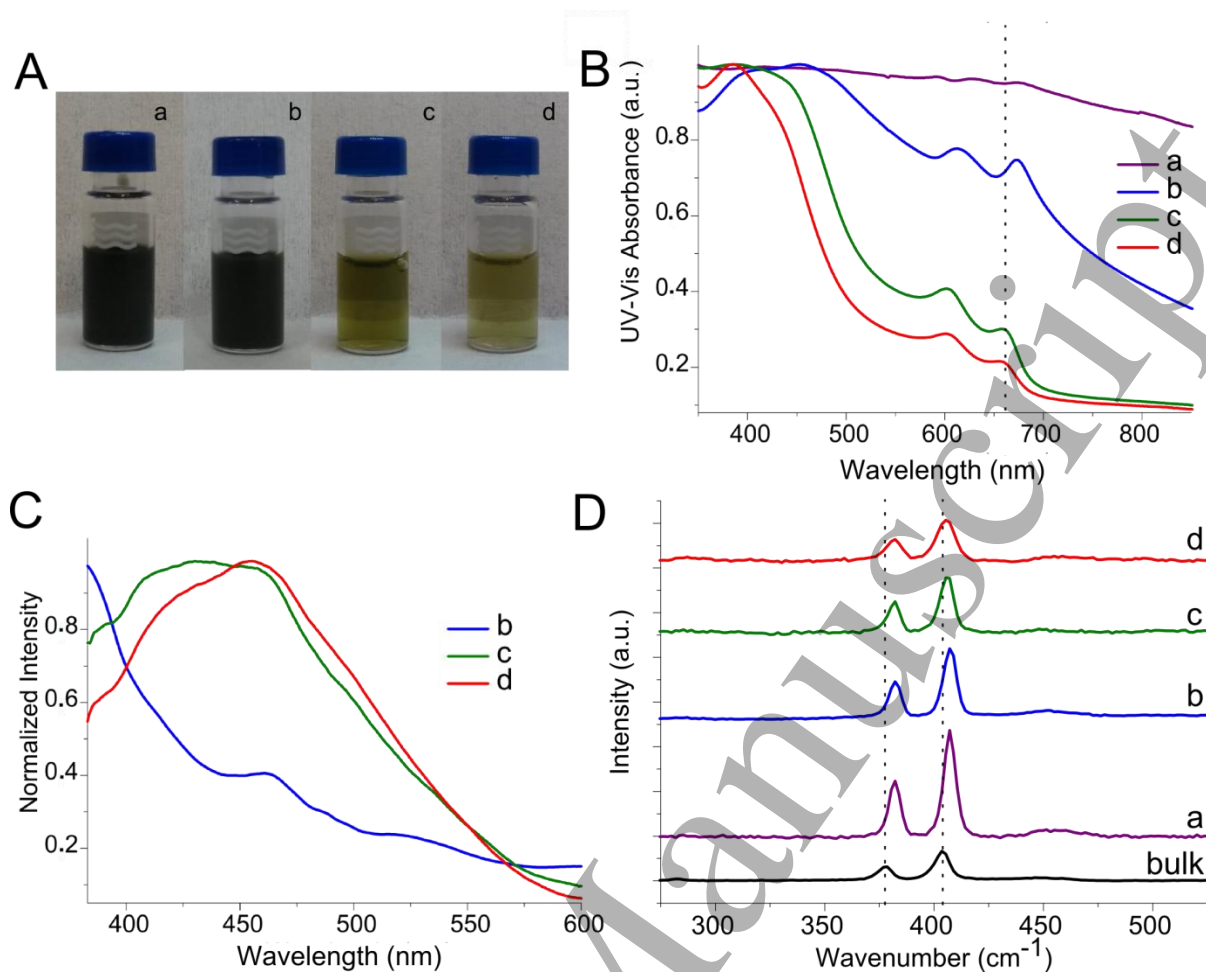
13 We performed the same set of experiment using a different starting material, such as graphite, to  
14 demonstrate that the AP-LYS is able to stabilize in a simple way different kinds of two-dimensional  
15 materials (Figure S4). Also in this case, different analyses were performed to evaluate the optimal  
16 conditions needed to prepare a stable sample of graphene (Figures S4-S7). The exfoliation yield of  
17 graphite is dependent on the amount of starting material and of stabilizer, as shown in the Figure S4.  
18 So, since the starting material and also the lysozyme are low cost precursors, it is possible to increase  
19 the yield increasing their concentration. We obtained a high and significant concentration of graphene  
20 ( $628 \pm 10 \mu\text{g mL}^{-1}$ ) decorated with positive charge (+32 mV) due to the AP-LYS coating (Figure S5).  
21 The exfoliation of graphite was confirmed by SEM images and Raman spectroscopy (Figures S6-S7).  
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### 29 **Production and stabilization of MoS<sub>2</sub> by AP-LYS**

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31 The exfoliated material obtained using the optimal experimental conditions as described in the  
32 previous section was thoroughly characterized. When the exfoliation, attempted in the absence of  
33 protein, produced a dark dispersion, that resulted clear without any detectable MoS<sub>2</sub>, after gentle  
34 centrifugation (see Figure S8).  
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37 Figure 4A shows the dispersions obtained after exfoliation (called JP, just prepared) and after  
38 centrifugation at different centrifugal force 40 g (called LM, low MoS<sub>2</sub>), 2500 g (called MM, medium  
39 MoS<sub>2</sub>) and 4500 g (called HM, high MoS<sub>2</sub>). Thanks to the centrifugation process we separate the  
40 MoS<sub>2</sub> classes.  
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44 The colour of dispersion changed from dark greenish to a yellowish suspension, indicating that the  
45 concentration decreased increasing the centrifugal force and in the same time the sample reached a  
46 smaller size (Figure 4A).  
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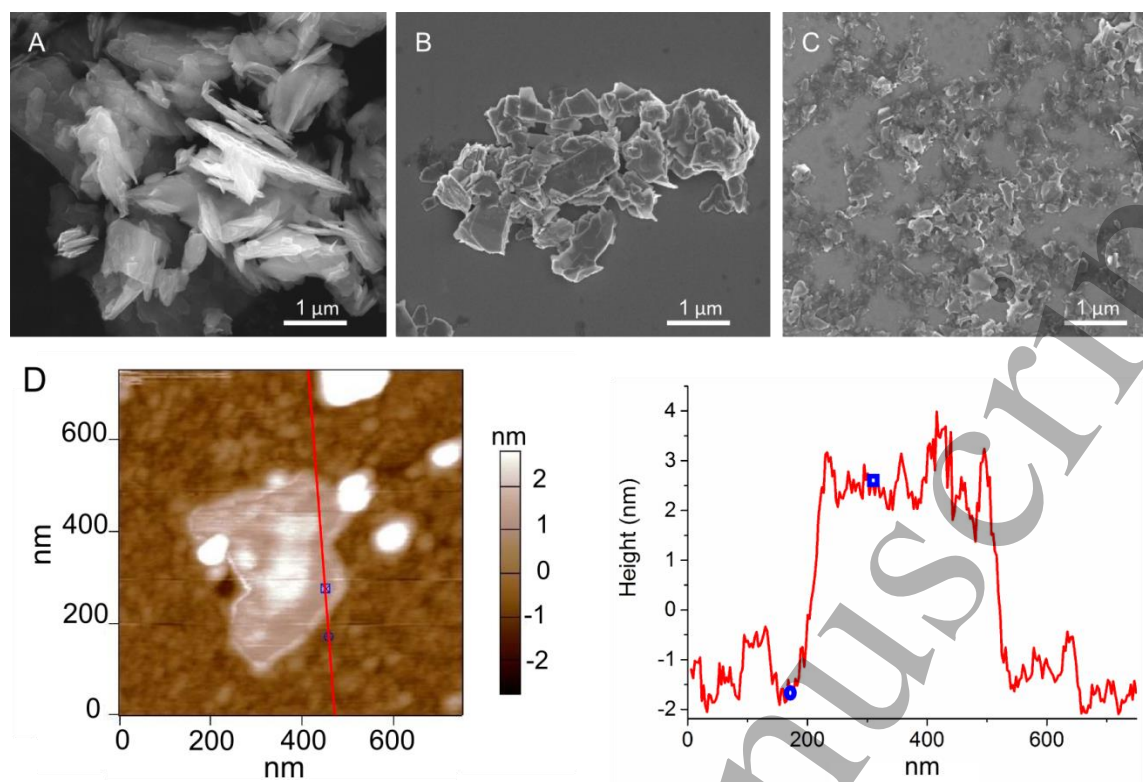


**Figure 4.** Production and characterization of biofunctionalized MoS<sub>2</sub> in the optimal condition. A) Liquid-phase exfoliation of (10mg) MoS<sub>2</sub> in the presence of (1 mg) AP-LYS. B) Absorption spectra of samples obtained at different centrifugal force C) Photoluminescence spectra (excitation at 342nm). D) Raman spectra of dispersions. a: JP, b: LM, c: MM, d: HM

SEM imaging was used to characterize the morphology of the starting material and that of the MoS<sub>2</sub> delaminated in presence of AP-LYS. The starting material was characterized by the presence of crystallites of 1-2  $\mu\text{m}$  lateral size (Figure 5A). Exfoliated material showed, with the increase of centrifugal force, a gradual decrease in the particle size (Figure 5B-C).

Accepted





**Figure 5.** Morphology of material. A) SEM image of the starting material. B) SEM image of the dispersion JP shown in (3A, a). C) SEM image of the dispersion LM shown in (3A, b). D, left) AFM analysis of exfoliated MoS<sub>2</sub> obtained in the dispersion HM shown in (3A, d). D, right) AFM profile of a flake.

The UV-Vis absorption spectra showed a progressive blue-shift of the peak at 687, typical of bulk MoS<sub>2</sub> from the JP to the HM dispersion due to a decrease in the number of layers (Figure 4B) [38, 61]. The MM and HM dispersions showed a narrowed main peak centered at 387 nm and a minor peak at 666 nm typical of single layer MoS<sub>2</sub> nanosheet [30,63]. The average number of layers present in each population, calculated as described previously [63,64], progressively decreased from 9.6 in the LM sample to 1.3 in the HM sample (Table S2). As expected, increasing the centrifugal force, the yield in the exfoliation dramatically decreased from 18.05 to 0.196 O.D (Table 1), obtaining MoS<sub>2</sub> of 180 μg mL<sup>-1</sup> (HM sample).

All dispersions showed a positive ζ-potential due to the adsorption of the cationic protein to the surface. Very interestingly, the highest value was measured for the HM sample. To further confirm the cationic nature of the exfoliate material, we also characterized the electrokinetic behaviour of LM, MM and HM. All the samples migrated toward the negative electrode with electrophoretic mobility (Ue) of  $1.984 \pm 0.137 \mu\text{m s}^{-1} \text{cm V}^{-1}$ ,  $2.104 \pm 0.088 \mu\text{m s}^{-1} \text{cm V}^{-1}$  and  $2.249 \pm 0.323 \mu\text{m s}^{-1} \text{cm V}^{-1}$  in the case of for LM, MM and HM samples, respectively. The progressive increase of the electrophoretic mobility is in good agreement with the ζ-potential values (Table 1, Figure S9). Since the protein is positive and the MoS<sub>2</sub> surface is nonpolar this charge is due to their assembling through

the adsorption of charged AP-LYS molecules onto the MoS<sub>2</sub> surface. Furthermore, the LM, MM and HM samples showed a progressively increasing photoluminescence emission at 455 nm (Figure 4C).

**Table 1. Stability, electrophoretic mobility and absorbance of MoS<sub>2</sub> dispersions**

Centrifugal Force (g)	ζ -Potential (mV)	Electrophoretic Mobility (μm s <sup>-1</sup> cmV <sup>-1</sup> )	Absorbance at 666nm (O.D.)
40	25.3 ± 1.8	1.984 ± 0.137	18.05 ± 1.23
2500	26.8 ± 1.1	2.104 ± 0.088	0.399 ± 0.025
4500	28.7 ± 2.9	2.249 ± 0.323	0.196 ± 0.001

We also characterized the Raman spectrum of the studied dispersions (Figure 4D). From the bulk material to the HM sample, we measured a red shift of the two bands E<sub>2g</sub><sup>1</sup> and A<sub>1g</sub>, respectively associated with the in-plane vibration and out-of-plane vibration, from 379 and 404 cm<sup>-1</sup> to 382 and 405 cm<sup>-1</sup> [39,65]. The red shift of E<sub>2g</sub><sup>1</sup> band is indicator of a reduction in the number of layers [2,66], however, the Raman spectrum of mechanically exfoliated MoS<sub>2</sub> monolayers usually show a blue shift of the A<sub>1g</sub> band instead of the red shift we observed. A possible explanation of this difference is that, differently from the E<sub>2g</sub><sup>1</sup> band, the A<sub>1g</sub> band is strongly influenced by surface adsorption and electron doping events and can even undergo a red shift depending on the environment conditions [2,39,67]. Therefore, the observed red shift could be caused by the adsorption of AP-LYS at the surface of the layers.

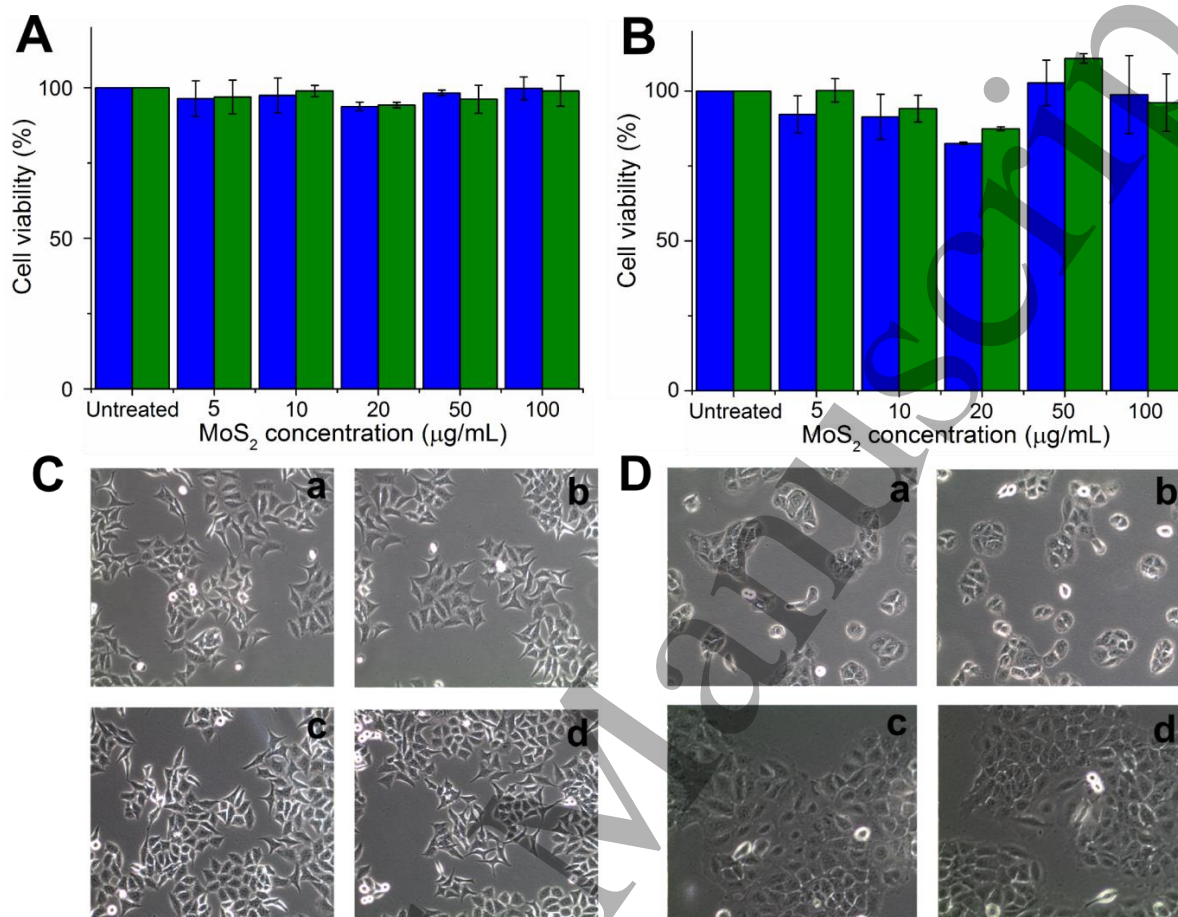
Additionally, atomic force microscopy confirmed the production of MoS<sub>2</sub> flakes with a thickness of 5nm (see Figure 5D and S10). On the basis of the lysozyme height obtained through the AFM analysis (Figure S11) we could assess that, in agreement with the results obtained from the UV-Vis analysis, the exfoliation process gave rise to monolayer MoS<sub>2</sub> nanosheets with lysozyme adsorbed onto both surfaces of the flakes. Moreover, the statistical analysis of the lateral size showed that most of the flakes had lateral sizes between 250 and 550 nm (Figure S12).

### Biocompatibility

In order to analyse the biocompatibility of MoS<sub>2</sub>, the stability of the HM sample in physiological conditions was evaluated by monitoring its UV-Vis after 48 hours incubation time (Figure S13). No difference was observed in the peak at 666 nm of the sample incubated in PBS buffer, 10 % FBS in 10 mM NaAc pH 5.0 or 10 % FBS in PBS buffer (Figure S13), thus suggesting that neither PBS nor FBS induce a significant alteration in the stability of the AP-LYS coated flakes.

Therefore, the biocompatibility of the HM sample was analysed using two model human cell lines, human cancer epithelial cells (HeLa cells) and human normal keratinocytes (HaCaT cells). The cells were treated with increasing amounts of the HM sample (from 5 to 100 μg mL<sup>-1</sup>) for 24 and 48 hours.

As shown in Figure 6A-B, cell viability was not affected at any of the concentration tested, up to 48 h incubation ( $p > 0.05$ ). Moreover, the cells did not show any change in their morphology (Figure 6C-D), thus indicating that this new material was completely biocompatible.



**Figure 6.** Biocompatibility of the HM dispersion using Alamar Blue assay and Cell imaging. on HeLa (blue bars) and HaCaT (green bars) cells at A) 24 hours and B) 48 hours. C) HeLa cells and D) HaCaT cells treated for 0 (a,b) and 48h (c,d) with 0 (a,c) and 20 µg/mL of HM sample (d). The images were recorded using a phase contrast microscope. All images were acquired at the same magnification.

In order to highlight the better efficiency of AP-LYS to biofunctionalize MoS<sub>2</sub> in aqueous solution, we compared our results with those obtained by Guan et al. (2015) [39] using BSA (Table S3). Even if both proteins are able to exfoliate MoS<sub>2</sub>, the procedures show several differences in terms of exfoliation time, yield and production rate. We produced 430 µg mL<sup>-1</sup> of MoS<sub>2</sub> after a sonication for 7 h, resulting in a yield of 21.5%, this value is lower than that obtained by Guan et al. (1360 µg mL<sup>-1</sup>, 27.2 %). In contrast, when we compare the exfoliation rate, we reached a production rate that is six times higher in order of magnitude (61.4 µg mL<sup>-1</sup> h<sup>-1</sup>). Furthermore, the concentration of AP-LYS is five times lower than that used by Guan et al. Moreover, using AP-LYS, the ratio between starting material and protein (MoS<sub>2</sub>: protein) is two times lower than the other one. This behaviour is due to

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3 the nature of denatured protein that has all residues exposed to the surface, thus it can interact with  
4 MoS<sub>2</sub> surface in excellent way. Finally, we found that the exfoliated material we obtained had no  
5 effect on cell viability (100% cell survival) up to 48h incubation and to 100 µg mL<sup>-1</sup>, with respect to  
6 Guan, who found a 30% of cell death after 24h with 10 µg mL<sup>-1</sup>. These differences are due to the  
7 unfolded nature of AP-LYS; while conventional 3D proteins, like BSA, have the hydrophobic  
8 residues in the core, exposing the hydrophilic residues [21], on the contrary, denatured lysozyme  
9 totally exposes the hydrophobic groups, increasing the surface area and the flexibility thus optimizing  
10 the interaction with the MoS<sub>2</sub> surface. Moreover, thanks to this modification, AP-LYS enhances in  
11 terms of positive charge surrounding the material surface, which is useful for the binding of negatively  
12 charged agents, such as DNA, RNA, antibody, or other materials, such as gold nanoparticle. These  
13 advantages make denatured lysozyme a very promising bio-tool for the functionalization of MoS<sub>2</sub> and  
14 other 2D materials.  
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## 24 **Conclusions**

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26 We demonstrated a simple approach to exfoliate MoS<sub>2</sub> in aqueous media through the use of  
27 biofunctionalization agent (AP-LYS), making it biocompatible and useful for bio-applications. We  
28 proved that this method can be applied to different starting materials, such as graphite and  
29 molybdenum disulphide, using AP-LYS. Given the exposure of hydrophobic groups, AP-LYS is and  
30 advantageous biomaterial to stabilize and functionalize MoS<sub>2</sub>, obtaining high quality MoS<sub>2</sub> flakes.  
31 Furthermore, by centrifuging the sample at different centrifugal force it is possible to select MoS<sub>2</sub>  
32 classes with different layers. Thanks to AP-LYS coating, we produced highly stable and  
33 biocompatible MoS<sub>2</sub> dispersions with a positive charged providing an optimal surface for a wide  
34 range of applications with interest for applications in bionanotechnology and biomedicine. Overall,  
35 this approach allows for the production of different bio-hybrid materials, opening the way for the  
36 development and production of other remarkable biocompatible 2D materials.  
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52 Catalunya (Grant 2014 SGR 260).  
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